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## BLOOD VESSEL SEGMENTATION

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**Abstract:** The blood vessel segmentation is an important issue for assessing retinal abnormalities and diagnoses of many diseases. The segmentation of vessels is complicated by huge variations in local contrast, particularly in case of the minor vessels. In this paper, proposed a new method of texture based vessel segmentation to overcome this problem. It uses Gaussian and L\*a\*b\* perceptually uniform color spaces with original RGB for texture feature extraction on retinal images. A bank of Gabor energy filters are used to analyze the texture features from which a feature vector is constructed for each pixel. The Fuzzy C-Means (FCM) clustering algorithm is used to classify the feature vectors into vessel or non-vessel based on the texture properties. After the FCM clustering output it attains the final output segmented image after a post processing step.

**Keywords:** Medical Images; Texture Classification; Gabor Energy Filter Bank; FCM Clustering; Image Segmentation.

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## INTRODUCTION

The detection of blood vessels is very important as ophthalmologists can potentially screen larger populations for vessel abnormalities. In contrast, manual delineation of vessels becomes tedious or even impossible when the number of vessels in an image is large or when a large number of images are acquired. Blood vessel appearance can provide information on pathological changes caused by some diseases including diabetes, hypertension, and arteriosclerosis. Changes in retinal vasculature, such as hemorrhages, angiogenesis; increases in vessel tortuosity, blockages and arteriolar-venular diameter ratios are important indicators of, for example, diabetic retinopathy, and retinopathy of prematurity and cardiovascular risk. Information about blood vessels in retinal images can be used in grading disease severity or as part of the process of diagnosis of diseases.

Retinal segmentation is complicated by the fact that the width of the retinal vessels can vary from large to very small, and the local contrast of vessels is unstable, especially in unhealthy retinal images. Although a large number of schemes have been proposed for the detection of blood vessels, a huge improvement in detection procedures remains a necessity for the detection of minor vessels.

In this report novel approach is proposed for vessel segmentation which is equally efficient to detect major and minor vessels. It considers Gaussian and  $L^*a^*b^*$  perceptually uniform color spaces with the original RGB image for texture feature extraction. To extract features, a bank of Gabor energy filters with three wavelengths and twenty-four orientations is applied in each selected color channel. Then a texture image is constructed from the maximum response of all orientations for a particular wavelength in each color channel. From the texture images, a feature vector is constructed for each pixel. These feature vectors are classified using the FCM clustering algorithm. Finally, it segments the image based on the cluster centroid value.

## II. LITRETURE SURVEY.

There are different methods and techniques available to classify vessels from retinal images. Among all some methods are given in following table.

	Title	Author	Description
1	Retinal vessel extraction by matched filter response with first order derivative of, Fakhri karry. Gaussian.	Bob Zhang, Lin Zhang, Lei Zhang	The propose MF-FDOG is compose of original MF which is zero mean Gaussian function and first order derivative of Gaussian. The Vessel is detected by Thresholding the retinal images response to the MF.
	On the adaptive detection of blood vessel in retinal image. Liu.	Di Wu, Ming Zhang , Jyh-charn	It as adaptive detection scheme for large and small blood vessel in color retinal images Consisting three functions adaptive contrast enhancement, feature extraction of blood vessel and tracing. The average of 75% of small vessels was capture by this method.

*A. Retinal vessel extraction by matched filter response with first order derivative of gaussian.*

Accurate extraction of retinal blood vessels is an important task in computer aided diagnosis of retinopathy. The matched filter (MF) is a simple yet effective method for vessel extraction. However, a MF will respond not only to vessels but also to non-vessel edges. This will lead to frequent false vessel detection. In this paper proposed a novel extension of the MF approach, namely the MF-FDOG, to detect retinal blood vessels. The proposed MF-FDOG is composed of the original MF, which is a zero- mean Gaussian function, and the first-order derivative of Gaussian (FDOG). The vessels are detected by thresholding the retinal image's response to the MF, while the threshold is adjusted by the image's response to the FDOG. The proposed MF-FDOG method is very simple; however, it reduces significantly the false detections produced by the original MF and detects many fine vessels that are missed by the MF. It achieves competitive vessel detection results as compared with those state-of-the-art schemes but with much lower complexity. In addition, it performs well at extracting vessels from pathological retinal images.

*B. On the adaptive detection of blood vessel in retinal image.*

An adaptive detection scheme for large and small blood vessels in color retinal images. The scheme consists of three functions: adaptive contrast enhancement, feature extraction of blood vessels, and tracing. The average performance of method over twenty tested images is 84.3%

for truepositive rate (TPR), and 3.9% for false positive rate (FPR). For normal images, the TPRs range from 80%to 91%, and their corresponding FPRs range from 2.8% to 5.5%. For abnormal images, the TPRs range from 73.8% to 86.5% and the FPRs range from 2.1% to 5.3%, respectively. Small vessels take up 42% of overall vessel pixels, where 75% of small vessels were captured by our method. Enhancement of blood vessels is achieved from the extension of the adaptive histogram equalization technique. Feature extraction of small blood vessels is by using the standard deviation of Gabor filter responses along different orientations. Tracing of the vascular network consists of three major functions: *forward detection*, *backward verification*, and *bifurcation detection*. Combining extrapolation and local greedy search reduces the prediction errors of vessel directions by 15-20%. Only two sample images and their hand-traced maps are needed for parameter training and calibration.

### III. PROPOSED METHOD

Here a new method is proposed for blood vessel segmentation which is based on the texture property analysis of vessel and non-vessel parts in the color retinal images. The reasons are as follows. Firstly, due to large variation of local contrast in the retinal image, texture analysis is more appropriate to extract features from vessel and non-vessel parts in the retinal images. Secondly, a color texture is a patio-chromatic pattern and can be defined as the "distribution of colors over a surface"; therefore, incorporating color into texture analysis is enhancing the procedure. The original retinal images are in RGB color space which is not perceptually uniform and Euclidean distances in 3D RGB space do not correspond to differences as perceived by humans. In addition, perceptually uniform color spaces are very effective in rotation invariant color texture analysis. So, here perceptually uniform color spaces along with original RGB color channels are used to extract texture features.

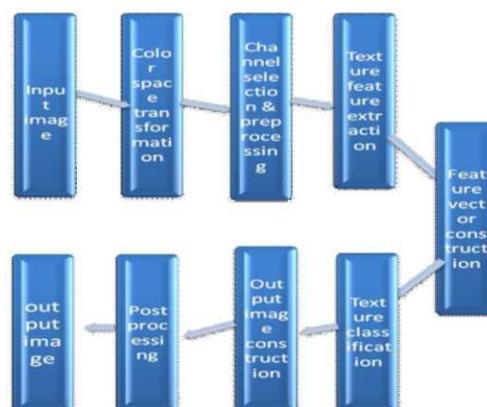


Fig.3.1. The vessel segmentation model.

At first apply the transformation of original RGB image into Gaussian and  $L^*a^*b^*$  color space. Then choose first two components of Gaussian color space "E and  $E^X$ , Luminance L from  $L^*a^*b^*$  color space and Green channel G from RGB color space due to the higher contrast of vessel and background which is convenient for texture analysis. After this apply Adaptive

Histogram Equalization (AHE) method to these four different color channel images for contrast enhancement. For each of these color channels, apply a bank of Gabor filters with twenty-four orientations and three wavelengths for texture feature extraction. Then construct the texture image in each color channel for every wavelength considering the maximum response of all twenty-four orientations. These texture images are used to analyze the number of clusters which latter will be used as the classifier input. Consequently, we construct twelve texture images for each original retinal image.

Here a feature vector for every pixel mapping each pixel position of all these texture image constructed (i.e. each feature vector is in the length of twelve elements). These feature vectors are classified as a vessel or background part using unsupervised FCM clustering algorithm. From the output of the FCM clustering algorithm construct a 2D matrix (as original image dimension) with cluster numbers which have the highest membership values (for each position). Finally, it produces the ultimate segmented image with converting the cluster numbers into binary values considering the cluster centroid values. Figure 3.1 portrays the overall technique of our proposed method.

#### A. Channel selection.

First apply the transformation of original RGB image into Gaussian and  $L^*a^*b^*$  color space. Then choose first two components of Gaussian color space "E and  $ETX$ , Luminance L from  $L^*a^*b^*$  color space and Green channel G from RGB color space due to the higher contrast of vessel and background which is convenient for texture analysis. Here for simplicity we have used only one color channel i.e. green. The green channel possess high contrast level which will be helpful in further processing.

#### B. Texture features extraction

Texture generally describes second order property of surfaces and scenes, measured over image intensities. A Gabor filter has weak responses along all orientations on the smooth (background) surface. On the other hand, when it positioned on a linear pattern object (like a vessel) the Gabor filter produces relatively large differences in its responses when the orientation parameter changes [2]. Hence, the use of Gabor filters to analyze the texture of the

retinal images is very promising. In the following two subsections the Gabor filter based texture analysis method.

•S'i layer			
Scale band *5>	• filter-size	Gabor	Gabor
Band 1	[1] 7 x 7 9x9	2-8 3.6	[2] 3.5 4.6
Band 2	[3] 11 x 11 13 x 13	4.5 5.4	[4] 5.6 6.8
Band 3	[5] 15 x 15 17 x 17	6.3 7.3	[6] 7.9 <>. 1
Band 4	[7] 19 X 19 21 x 21	8.2 9.2	[8] 11.1.3 11.5
Band 5	[9] 23 x 23 25 ■ 25	10.2 11.:	[10] 12.7 14.1
Band 6	[11] 27 X 27 20 x 29	12.3 13.4	[12] 15.4 16.8
Band 7	31 X 31 33 x 33	14.6 15.8	[13] 18.2 19.7
Band 8	[14] 35 x 35 37 x 37	17.0 18.2	[15] 21.2 22.8

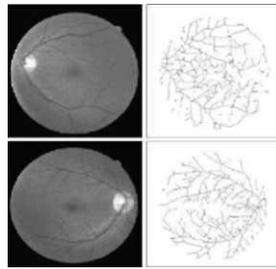
**Fig 3.2 table of Gabor filter bank**

*C. TEXTURE CLASSIFICATION AND IMAGE SEGMENTATION* The FCM is a data clustering technique where in each data point belongs to a cluster to some degree that is specified by a membership grade. Let  $X = \{x_1, x_2, \dots, x_n\}$  where  $x \in \mathbb{R}^N$  present a given set of feature data. The objective of the

FCM clustering algorithm is to minimize the Fuzzy C-Means cost function formulated as

$$J(U, V) = \sum_{p,j} \sum_{i=1}^N u_{pj}^m \|x_i - v_j\|^2$$

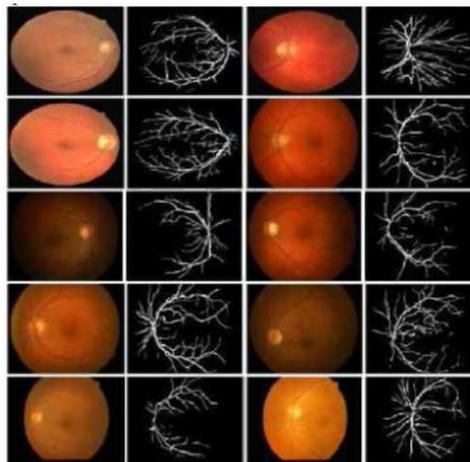
$V = \{v_1, v_2, \dots, v_C\}$  are the cluster centers.  $U = (u_{pj})_{N \times C}$  is fuzzy partition matrix, in which each member is between the data vector  $x_i$  and the cluster  $J$ . The values of matrix  $U$  should satisfy the following conditions:  $u_{pj} \in [0, 1], \sum_{j=1}^C u_{pj} = 1, \forall i = 1, \dots, N$



**Fig. 3.3 Original images (left) and segmented vessel center line images (right).**

The exponent  $m \in [1, \infty]$  is the weighting exponent, which determines the fuzziness of the clusters. The most commonly used distance norm is the Euclidean distance  $d_{ij} = \|x_i - v_j\|$ .

The Matlab Fuzzy Logic Toolbox is used for clustering 253440 vectors (the size of the retinal image is 512x495) in length twelve for each retinal image. In each retinal image clustering procedure, the number of clusters was assigned after analyzing the histogram of the texture image. The parameter values used for the FCM clustering were as follows. The exponent value of 2 for the partition matrix, maximum number of iterations was set to 1000 for the stopping criterion and the minimum amount of improvement being 0.00001. Here the membership values on each cluster for every vector are received, from which the cluster number that belonged to the highest membership value for each vector are taken out and converted it into a 2D matrix. From this matrix produced the binary image considering the cluster central intensity value which identifies the blood vessels only.



**Fig 3.4. Results for random samples of Original and Segmented Images.**

## EXPERIMENTAL RESULTS

In this project segmented vessel are found from color retinal images with software approached. The output image of fundus camera is directly inputted to the process and after processing output image is segmented image of vessel. This method is very useful to find smallest blood vessel from the color retinal image. The segmented blood vessel appearance can provide information on pathological changes caused by some diseases example diabetes, hypertension, and arteriosclerosis.

## IV. CONCLUSION

In this project proposed a novel approach for a texture based vessel segmentation technique. The automated vessel detection reduces manual delineation. This method is very efficient in detecting both major and minor blood vessels.

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